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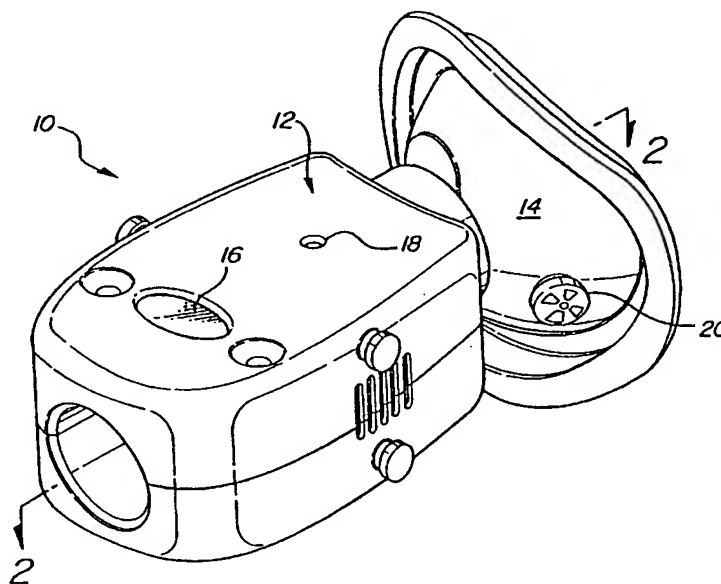
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(54) Title: RESPIRATORY NITRIC OXIDE METER



(57) Abstract: A respiratory nitric oxide meter (10) includes a respiratory connector (14) designed to be supported in contact with a subject and to pass respiratory gases as the subject breathes. A flow pathway (20) receives and passes the respiration gases. One end of the pathway (20) is in fluid communication with the respiratory connector (14), and the other end is in fluid communication with a reservoir of respiratory gases. A nitric oxide concentration sensor (24) generates electrical signals as a function of the instantaneous fraction of nitric oxide as the respiration gases pass through the flow pathway (20).

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RESPIRATORY NITRIC OXIDE METER

Field of Invention

The present invention relates generally to the detection of nitric oxide in a gaseous mixture and, more specifically, to the detection of nitric oxide in a flow pathway.

Background of the Invention

DEFINITION OF NITRIC OXIDE:

Nitric oxide, NO, is a colorless gas useful in the detection and treatment of a variety of medical conditions such as asthma. Nitric oxide, NO, should not be confused with nitrous oxide, N₂O, or nitrogen dioxide, NO₂. Nitrogen and oxygen also form other compounds, especially during combustion processes. These typically take the form of NO_x where x represents an integer. These forms are generally referred to as NO_x. Detection of nitric oxide, NO, is the primary focus of the present application. Nitric oxide has a variety of beneficial uses and detection of nitric oxide, especially in small concentrations, is necessary for the proper administration of nitric oxide and diagnosis of disease.

USE OF NITRIC OXIDE IN TREATMENT OF PHYSIOLOGICAL CONDITIONS

Nitric oxide is beneficial in both the treatment and diagnosis of asthma and other forms of lung disorders. Asthma is a chronic disease characterized by intermittent, reversible, widespread constriction of the airways of the lungs in response to any of a variety of stimuli that do not affect the normal lung. A variety of drugs are commonly used to treat asthma. It is known that inhalation of nitric oxide

(NO) is therapeutically beneficial in the prevention and treatment of asthma attacks and other forms of bronchoconstriction, of acute respiratory failure, or of reversible pulmonary vasoconstriction as discussed in U.S. Patent No. 5,873,359 to Zapol et al, incorporated herein by reference. U.S. Patent Nos. 5,904,938 and 6,063,407, both to
5 Zapol et al. and incorporated herein by reference, disclose the use of inhaled nitric oxide in the treatment of vascular thrombosis and retinosis. Typically, treatment utilizing nitric oxide includes the introduction of nitric oxide as a portion of the respiratory gases being inhaled by the patient. The nitric oxide concentration is usually in the range of 1 to 180 parts per million (ppm). The difficulty presented in
10 the administration of controlled amounts of nitric oxide is the determination of the concentration being introduced. It has traditionally been very difficult to quickly and accurately determine the concentration of nitric oxide in the gas mixture, especially where the concentration of nitric oxide is very low.

U.S. Patent No. 5,839,433 to Higenbottam, incorporated herein by reference,
15 describes the use of nitric oxide in the treatment of certain lung diseases and conditions. As discussed in the specification, a drawback to the administration of gaseous nitric oxide is that it rapidly converts to nitrogen dioxide, a potentially harmful substance. Consequently, it is often preferable to intubate the patient so that nitric oxide is administered directly to the lungs. Whether or not intubated, it is very
20 important to accurately monitor the amount of nitric oxide being introduced to the lungs. The Higenbottam reference proposes an improvement wherein the nitric oxide is introduced as a short pulse of known volume, rather than continuously during inhalation.

U.S. Patent No. 5,531,218 to Krebs, incorporated herein by reference, discusses the benefits of nitric oxide inhalation in the treatment of various disorders, including adult respiratory distress syndrome, (ARDS). The specification discloses a system for administering nitric oxide that includes a source of nitric oxide, an analyzer for analyzing nitric oxide concentration, and a control unit, with the analyzer and the control unit cooperating to maintain the appropriate nitric oxide concentration. However, this system relies on the use of nitric oxide sensors utilizing infrared absorption measurement, electrochemical sensors, or chemiluminescence detectors. Each of these analyzers have drawbacks and cannot provide instantaneous nitric oxide concentration measurements.

USE OF NITRIC OXIDE IN DIAGNOSIS

Nitric oxide may also be used in the diagnosis of various physiological conditions. For example, the reversibility of chronic pulmonary vasostriction may be diagnosed by administering known quantities of nitric oxide and monitoring changes in pulmonary arterial pressure (PAP) and cardiac output as described in US Patent No. 5,873,359 to Zapol et al.

Endogenous production of nitric oxide in the human airway has been shown to be increased in patients with asthma and other inflammatory lung diseases. Expired nitric oxide concentrations are also elevated in patients with reactive airways disease. Therefore, detection of nitric oxide is beneficial in diagnosing these conditions. However, proper diagnosis requires accurate measurement of nitric oxide in parts per billion (ppb) of gas-phase nitric oxide.

Determination of the level of nitric oxide is useful in the diagnosis of inflammatory conditions of the airways, such as allergic asthma and rhinitis, in

respiratory tract infections in humans and Kartagener's syndrome. It also has been noted that the level of nitric oxide in the exhalation of smokers is decreased. U.S. Patent No. 5,922,610 to Alving et al., incorporated herein by reference, discusses the detection of nitric oxide in diagnosing these conditions, as well as gastric
5 disturbances.

In addition to the above, nitric oxide may be used in the determination of lung function. For example, U.S. Patent No. 5,447,165 to Gustafsson, incorporated herein by reference, explains that nitric oxide in exhalation air is indicative of lung condition. As one test of lung function, a subject may inhale a trace gas, such as nitric
10 oxide. Then the concentration and time-dispersment of the gas in the exhalation air is measured. The shape of the curve representing the time dependent gas concentration in the exhalation air is indicative of lung function or condition. Obviously, it is necessary to have an accurate determination of both the concentration and the time-dependence of the concentration to allow for the most accurate diagnosis.

15 During exhalation, gas mixture changes during the breath. The initial portion of the exhalation is "dead space" air that has not entered the lungs. This includes the respiratory gases in the mouth and respiratory passages above the lungs. Also, some portion of the exhalation measured by an analytical instrument may be attributed to dead air in the mask and flow passages of the apparatus. As a breath continues,
20 respiratory gases from within the lungs are exhaled. The last portion of respiratory gases exhaled is considered alveolar air. Often it is beneficial to measure gas concentrations in alveolar air to determine various pulmonary parameters. For example, nitric oxide, as an indicator of various disease states, may be concentrated in the alveolar air. However, nitric oxide is also produced by various mucus membranes

and therefore nitric oxide may be present in both the dead air space and in the alveolar air. During an exhalation, the dead air space may be overly contaminated with nitric oxide due to residence in the mouth and nasal cavities where nitric oxide is absorbed from the mucus membranes. Therefore, it is necessary to distinguish the various portions of exhalation for proper diagnosis. U.S. Patent No. 6,038,913 to Gustafsson et al., incorporated herein by reference, discusses having an exhalation occur with very little resistance during an initial "dead space" phase of exhalation and then creating resistance against the remaining portion of the exhalation.

NITRIC OXIDE MEASUREMENT METHODS

10 Numerous approaches have been used and proposed for monitoring the concentration of nitric oxide in a gas mixture. These include mass spectroscopy, electrochemical analysis, colorimetric analysis, chemiluminescence analysis, and piezoelectric resonance techniques. Each of these approaches have shortcomings that make them poorly suited to widespread use in the diagnosis and treatment of disease.

15 Mass spectroscopy utilizes a mass spectrometer to identify particles present in a substance. The particles are ionized and beamed through an electromagnetic field. The manner in which the particles are deflected is indicative of their mass, and thus their identity. Mass spectroscopy is accurate but requires the use of very expensive and complicated equipment. Also, the analysis is relatively slow, making it
20 unsuitable for real time analysis of exhalations. Preferably, in the breath by breath analysis of nitric oxide, it is desirable to quickly and accurately measure the nitric oxide concentration in the flow path as the gas mixture flows through the flow path. Mass spectroscopy requires sampling of portions of the gas mixture rather than analyzing the nitric oxide concentration in the flow pathway itself. Mass

spectroscopy cannot be considered an instantaneous or continuous analysis approach. It requires dividing the exhalation into multiple discrete samples and individual analysis of each sample. This does not create a curve of the nitric oxide concentration but instead creates a few discrete points. Sampling-based systems are especially
5 deficient when detecting gases in very low concentrations since large samples are required.

Electrochemical-based analysis systems use an electrochemical gaseous sensor in which gas from a sample diffuses into and through a semi-permeable barrier, such as membrane, then through an electrolyte solution, and then to one of typically
10 three electrodes. At one of the three electrodes, a sensing redox reaction occurs. At the second, counter, electrode, a complimentary and opposite redox reaction occurs. A third electrode is typically provided as a reference electrode. Upon oxidation, or reduction, of the nitric oxide at the sensing electrode, a current flows between the sensing and counter electrode that is proportional to the amount of nitric oxide
15 reacting at the sensing electrode surface. The reference electrode is used to maintain the sensing electrode at a fixed voltage. A typical electrochemical-based gas analyzer for detecting nitric oxide is shown in U.S. Patent No. 5,565,075 to Davis et al, incorporated herein by reference. Electrochemical-based devices have high sensitivity and accuracy, but typically have a response time in excess of 30 seconds.
20 This is significantly too slow to allow breath by breath, or continuous, analysis of respiration gases.

Colorimetric analysis relies on a chemical reaction by a gas which provides a corresponding change in pH, thereby triggering a color change in an indicator. This approach requires expendable chemical substances. Also, this approach is often

disturbed by the presence of other gases, particularly the relative amount of humidity present. Response times are too slow for analysis during a breath.

Chemiluminescent-based devices depend on the oxidation of nitric oxide by mixing the nitric oxide with ozone, O_3 , to create nitrogen dioxide and oxygen. The
5 nitrogen dioxide is in an excited state immediately following the reaction and releases photons as it decays back to a non-excited state. By sensing the amount of light emitted during this reaction, the concentration of nitric oxide may be determined. An example of a chemiluminescent-based device is shown in U.S. Patent No. 6,099,480 to Gustafsson, incorporated herein by reference. Chemiluminescent devices have
10 response times as fast as about two hundred milliseconds, have high sensitivity, repeatability, and accuracy. However, like with mass spectroscopy, and electrochemical analysis, chemiluminescent analysis requires sampling of the gas mixture rather than continuous analysis of the gas concentration in the flow path itself. Also, chemiluminescent devices are typically very large and expensive.

15 Piezoelectric resonance techniques are sometimes referred to as MEMS (micro-electro-mechanical systems) sensor devices. Basically, a micro-etched cantilevered beam is coated with a "capture" molecule that is specific to the gas being analyzed. In theory, the capture molecule will capture the gas being analyzed in proportion to its ambient concentration. This alters the mass of the micro-etched
20 cantilevered beam. Changes in mass of the beam may theoretically be detected based on changes in its resonant frequency. The change in resonant frequency should be directly proportional to the concentration of the gas being studied. A system for detecting air pollutants is disclosed in U.S. Patent No. 4,111,036 to Frechette et al., incorporated herein by reference. While the theory behind piezoelectric resonance

techniques is rather simple, there has been no known success to date in the analysis of nitric oxide concentrations.

U.S. Patent No. 6,033,368 to Gaston IV et al. discloses an analyzer for measuring exhaled nitrogen oxides, nitrite and nitrate in very low concentrations. The analyzer includes a chilled exhalation passage which causes lung fluid vapors to collect. The resulting liquid is then analyzed using standard calorimetric assays. While somewhat simpler than other methods, the Gaston apparatus remains complicated, requiring pre-freezing of the chilling apparatus, and subsequent analysis of the collected liquid.

Each of the above-described approaches for the use and detection of nitric oxide would benefit from a nitric oxide meter capable of continuously determining the nitric oxide concentration of a flow of respiratory gases in a flow pathway without the need for sampling the mixture. Most preferably, such a meter would provide nearly instantaneous response times so that analysis may be made during a breath or on a breath-by-breath basis.

Summary of the Invention

The present invention overcomes many of the shortcomings of the prior art by providing a nitric oxide meter designed to provide continuous, or breath-by-breath, analysis. The nitric oxide meter includes a respiratory connector designed to be supported in contact with a subject so as to pass respiratory gases when the subject breathes. A flow pathway receives and passes respiration gases. One end of the flow pathway has in fluid communication with the respiratory connector, and the other end is in fluid communication with a source and sink of respiratory gases. A nitric oxide

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concentration sensor generates electrical signals as a function of the instantaneous fraction of nitric oxide in the respiration gases as the gases pass through the flow pathway. In some embodiments of the present invention, a flow meter is also provided in the respiratory nitric oxide meter. The flow meter may be an ultrasonic
5 flow meter including a pair of spaced-apart ultrasonic transducers. In other embodiments of the present invention, the respiratory nitric oxide meter forms part of a system for the controlled administration of nitric oxide to the subject. This system includes a nitric oxide regulator designed to selectively introduce nitric oxide into inhalation gases in the pathway. The system may also include a controller which
10 controls the regulator based on signals received from the nitric oxide concentration sensor so as to maintain the instantaneous fraction of nitric oxide in the inhalation gases within prescribed limits.

Brief Description of the Drawings

FIGURE 1 is a perspective view of the first embodiment of a respiratory nitric
15 oxide meter according to the present invention;

FIGURE 2 is a cross-sectional view of the meter of Figure 1 taken along lines
2-2;

FIGURE 3 is an exploded perspective view of an embodiment of a nitric
oxide sensor for use with a nitric oxide meter;

20 FIGURE 4 is a cross-sectional side view of the sensor of Figure 3 taken along
lines 4-4;

FIGURE 5 is a perspective view of a first alternative embodiment of a
respiratory nitric oxide meter according to the present invention;

FIGURE 6 is a perspective view of a second alternative embodiment of a nitric oxide meter according to the present invention;

FIGURE 7 is a cross-sectional view of the meter of Figure 6 taken along lines 7-7;

5 FIGURE 8 is a perspective view, partially exploded, of a third alternative embodiment of the nitric oxide meter according to the present invention;

FIGURE 9 is a view of a nitric oxide metering system according to the present invention with the meter portion shown in cross-section; and

10 FIGURE 10 is a schematic of a nitric oxide administration system utilizing a nitric oxide meter according to the present invention.

Detailed Description of the Preferred Embodiments

The present invention provides a respiratory nitric oxide meter that allows the measurement of the instantaneous nitric oxide concentration in a gaseous mixture as the mixture flows through a flow pathway. Unlike the prior art, the present invention is not a sampling based analyzer, but instead measures the concentration of nitric oxide in the flow pathway itself and has a sufficiently fast response time so as to allow analysis on a breath-by-breath basis and to allow the monitoring of the changes in nitric oxide concentration during a single breath. For the purposes of the present invention, the nitric oxide sensors used as part of the nitric oxide meter are considered instantaneous, with instantaneous being defined as fast enough to allow monitoring of changes in the nitric oxide concentration during a single breath. Investigation has indicated that response times of approximately 200 milliseconds (ms) or less are preferred in order to track changes in nitric oxide concentration, with 100 ms or less

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being even more preferred. Many of the prior art sensors and analyzers have response times on the order of several seconds, making them unsuitable for breath-by-breath analysis of the nitric oxide concentration of either inhalation or exhalation gases. Also, many are sampling based analyzers and therefore analyze discrete samples. The
5 present invention also allows close correlation between nitric oxide measurements and flow measurements, something not easily accomplished with prior art systems.

Referring to Figures 1 and 2, a first embodiment of a respiratory nitric oxide meter is generally shown at 10. The meter 10 includes a body 12 and a respiratory connector, such as a mask 14, extending from the body 12. Preferably, the meter 10 is
10 a lightweight, handheld or wearable unit. In use, the user grasps the body 12 and brings the mask 14 into contact with their face so that respiratory gases pass through the meter 10. Though not shown, straps may be provided for interconnecting the meter 10 with the user's face and head without the need to support it with a hand.

With the mask 14 in contact with the user's face, the user's inhalations and/or
15 exhalations pass through the body 12 for analysis of the nitric oxide concentration. The meter 10 preferably includes a display 16 as well as a control button 18 for controlling operation of the meter 10.

Depending on the application, the meter 10 may be used to pass inhalation gases, exhalation gases, or both. In situations where it is preferred to pass only
20 inhalation or exhalation gases, but not both, a valve 20 may be provided on the mask for allowing passage of the gases not to be analyzed. For example, the valve 20 may be one-way valve that allows the passage of fresh air into the mask 14 upon inhalation but blocks exhalation, such that exhalation gases pass through the body 12 of the meter 10. By reversing the valve 20, exhalations may be passed through the valve

while inhalations enter through the body 12. A second one-way valve may be provided in the body 12 for further directing gases. Without the valve 20, or with the valve disabled, both inhalation and exhalation gases pass through the body 12.

Referring now to Figure 2, the meter 10 is shown in cross-section so as to illustrate the internal construction. A flow pathway is formed through the body 12 by a generally straight flow tube 20. At one end, the flow tube 20 is interconnected with the mask 14, and its other end is open to the surrounding air. Alternatively, the second end of the flow tube may be interconnected with a source and/or sink of respiratory gases, which may be referred to as a reservoir of respiratory gases. The term "reservoir" may also refer to the surrounding air. The body 12 includes an outer shell 22 which surrounds the majority of the flow tube 20 so as to provide an improved cosmetic appearance and to support a variety of additional components. As shown, the flow tube 20 is a generally cylindrical tube with a generally constant cross-section throughout its length. Consequently, inhalation and exhalation gases flow very freely into and out of the mask 14, thereby creating little resistance to natural respiration. A nitric oxide sensor 24 is disposed in the side of the flow tube 20 so as to be in contact with respiratory gases passing through the flow tube. The sensor 24 has a sensing face 25 positioned in a window or opening in the side of the tube.

In some embodiments of the present invention, a flow meter is also provided so as to measure the flow of respiratory gases through the flow tube 20. Many types of flow meters may be used. However, in the preferred embodiment, an ultrasonic-based flow meter is used. Ultrasonic flow meters measure the instantaneous flow velocity of gas in a flow tube, thereby allowing determination of flow volumes. In the

embodiment shown in Figure 2, a pair of spaced-apart ultrasonic transducers 26 and 28 are disposed in the ends of a pair of side passages 30 and 32 which branch off of the flow tube 20. Ultrasonically transparent covers 27 may be provided where the side passages 26 and 28 intersect the flow tube 20 to reduce or prevent flow disturbances at the intersections. The ultrasonic transducers 26 and 28 and the side branches 30 and 32 are arranged such that ultrasonic pulses traveling between the transducers 26 and 28 pass through the flow tube 20 at an angle to its central axis. That is, ultrasonic pulses traveling between the transducers 26 and 28 travel along a path which is angled to the path of flow of respiratory gases through the flow tube 20.

As shown, the side passages 30 and 32 essentially form an interrupted tube which intersects the flow tube 20 at an angle. As will be clear to those of skill in the art, ultrasonic pulses traveling between the transducers 26 and 28 have a component of their direction of travel which is parallel to the direction of flow of respiratory gases through the flow tube 20.

Measurement of flow velocity using ultrasonic pulses is described in U.S. Patent Nos. 5,419,326; 5,503,151; 5,645,071; and 5,647,370, all to Harmoncourt et al, which are incorporated herein by reference. In the Harmoncourt patents, ultrasonic transducers are positioned so as to transmit pulses through a flowing fluid in a direction that has a component in the flow direction. Specifically, with fluid flowing through a tube, the transducers are positioned in the side walls of the tube at an angle such that ultrasonic pulses are transmitted at an angle to the fluid flow. Flow speed may be calculated based on the fact that ultrasonic pulses traveling with the flow travel faster while ultrasonic pulses traveling against the flow travel slower. Mathematical corrections are made for the fact that the ultrasonic pulses are traveling

at an angle to the flow. Preferably, pulses are alternately transmitted in a direction with the flow and in a direction against the flow so that a time difference may be calculated. The present invention may use ultrasonic transducers comprising a metalized polymer film and a perforated metal sheet. In one preferred embodiment,
5 the ultrasonic flow measurement system is supplied by NDD of Zurich, Switzerland and Chelmsford, MA.

Ultrasonic pulses are transmitted with and against the direction of flow, resulting in measurement of upstream and downstream transit times. If the gas flow rate is zero, the transit times in either direction through the gas are the same, being
10 related to the speed of sound and distance traveled. However, with gas flow present, the upstream transit times differ from the downstream transit times. For constant flow, the difference between sequential upstream and downstream transit times is directly related to the gas flow speed. Further details of this approach to ultrasonic flow sensing may be obtained by reference to Applicant's co-pending patent
15 application Serial No. 09/630,398, which is incorporated herein in its entirety by reference. Processing circuitry and additional sensors may be provided within the housing 12 for processing signals from the ultrasonic sensors 26 and 28, as also described in Applicant's co-pending application referred to above. Also, a fan 29 may be provided to force fresh air over some of the internal circuitry. As shown, the
20 nitric oxide sensor 24 is positioned in the wall of the flow tube 20 approximately midway between the ultrasonic transducers 26 and 28. Therefore, the same portion of the flow is measured for flow speed and nitric oxide concentration at the same time, allowing coordination of the data.

Referring now to Figures 3 and 4, one embodiment of a nitric oxide sensor 24 is shown. Preferably, instantaneous nitric oxide concentration is measured at the same time flow is measured. In the presently preferred embodiment of the present invention, a fluorescence-based nitric oxide sensor is used to determine the partial
5 pressure of nitric oxide in the respiration gases passing through the flow tube 20.

Fluorescence based oxygen sensors are known in the art, for example as described by Colvin (U.S. Patent Nos. 5,517,313; 5,894,351; 5,910,661; and 5,917,605; and PCT International Publication WO 00/13003, all of which are incorporated herein by reference). A sensor typically comprises an oxygen permeable
10 film in which oxygen-indicating fluorescent molecules are embedded. In Patent Nos. 5,517,313 and 5,894,351, Colvin describes sensors using a silicone polymer film, and suggests using a ruthenium complex, tris(4,7-diphenyl-1,10-phenanthroline)ruthenium (II) perchlorate, as the oxygen indicator fluorophore molecule. The orange-red fluorescence of this ruthenium complex is quenched by the local presence of oxygen.
15 Oxygen diffuses into the oxygen permeable film from the gas flowing over the film, inducing fluorescence quenching. The time response of the quenching effect, relative to concentration changes of oxygen in the gas outside the film, is related to the thickness of the film. Thin films are preferred for a rapid response, as described in 5,517,313.

20 Referring now to Figures 3 and 4, the fluorescence based nitric oxide sensor used in the present embodiment is shown generally at 24. Figure 3 is an exploded view and Figure 4 is a cross sectional view. The presently preferred sensor is based on the technology described in the Colvin patents but has a chemistry adapted to detection of nitric oxide. A circuit board 40 has a plurality of pins 42 extending

downwardly for interconnecting the sensor with other components. An LED 44 is mounted generally to the center of the top of the circuit board. A pair of photodiodes 46 and 48 are also mounted to the top of the circuit board. The photodiodes are mounted symmetrically on opposite sides of, and a short distance from, the LED 44.

5 An optical filter is mounted on top of each photodiode; filter 50 is mounted on photodiode 46 and filter 52 is mounted on photodiode 48. The optical filters preferably are bonded to the photodiodes with an optically clear adhesive.

A heat spreader 54, preferably a thin copper sheet with down-turned edges, is mounted to the top of the circuit board. The heat spreader has a downwardly
10 extending foot 56 at each of its four corners, each of which engage a hole 58 in the circuit board 40. The feet and the down-turned edges of the heat spreader 54 support the central portion of the heat spreader a short distance above the circuit board, leaving a gap therebetween. The LED 44, the photodiodes 46 and 48, and the filters 50 and 52 are disposed in this gap between the circuit board and the heat spreader.

15 Two round holes 60 are cut in the heat spreader, one hole being directly above each of the photodiodes 46 and 48. Two pieces of glass substrate 62 and 64 are mounted to the top of the heat spreader, with one piece being mounted directly on top of each of the holes 60. As shown, these pieces of substrate 62 and 64 are square. A circle of fluorescent film is formed on top of each of the pieces of substrate; film circle 66 is
20 formed on substrate 62 and film circle 68 is formed on substrate 64. A gas impermeable glass cover 70 is disposed over film circle 66 and bonded to the glass substrate 62 with epoxy 72. Therefore, film circle 66 is sealed in by the cover 70 above and the epoxy 72 at the edges. This results in one of the film circles, 68, being exposed to the surrounding atmosphere, while the other film circle, 66, is sealed in

and not exposed. Therefore, film circle 66 does not react to changes in nitric oxide concentration while film circle 68 does. Film circle 68 will be referred to as a sensing region and film circle 66 will be referred to as a reference region. The substrates 62 and 64 and the materials applied to them form the sensing face of the sensor.

5 Referring again to Figure 4, the gap between the circuit board 40 and the heat spreader 54, as well as the holes 60, are filled with an optically clear waveguide material 74. The waveguide material 74 serves to optically couple the LED 44 to the glass substrates 62 and 64, making the substrates an integral part of the waveguide. The waveguide material also optically couples the sensing region 68 and reference
10 region 66 to the filters 50 and 52 and the photodiodes 46 and 48. The result is a continuous optical waveguide that optically couples these components. Suitable waveguide materials are manufactured by Norland Products of New Brunswick, New Jersey, and by Epoxy Technology of Billerica, Massachusetts, the latter under the name EPOTEK®.

15 In order to avoid problems with condensation forming on the sensing region 68 and the reference region 66, the regions are preferably both warmed using the heat spreader 54. For this purpose, small heaters 76, comprising resistors, are mounted to the circuit board 40 adjacent each of the foot mounting holes 58. The heat spreader feet 56 are soldered into the holes, and to the heaters 76 so that heat is transferred into
20 the spreader. A thermistor 78 is mounted to the circuit board 40 in a position such that it contacts one of the down-turned edges of the heat spreader 54 when the sensor is assembled. The thermistor may be soldered to the edge to improve heat transfer. The thermistor is then used to monitor the temperature of the heat spreader, and the heaters are controlled so as to maintain a generally constant temperature. An

EEPROM, containing calibration data for the sensor, may be mounted to the underside of the circuit board.

The fluorescent films 66 and 68 are formed of materials whose fluorescence or absorbance characteristics change as a function of nitric oxide concentration. As an example, thiol or sulfhydryl may be joined to a fluorophore such as pyrene giving
5 sulfhydrylpyrene). In this respect, an article entitled "Determination of Nitric Oxide Levels by Fluorescence Spectroscopy" by G. Gabor and N. Allon, published in the *Biochemical, Pharmacological, and Clinical Aspects of Nitric Oxide* (Edited by B.A. Weissman et al., Plenum Press, New York, 1995) is incorporated herein in its entirety.

10 Radiation from the LED is transmitted to the sensing region 68 and the reference region 66 by the optical waveguide material 74. The wavelength emission of the LED 44 is chosen to induce fluorescence from the fluorescent film regions 66 and 68. Fluorescence emissions from the sensing and reference regions, preferably shifted in wavelength compared to the LED radiation, are detected by the two
15 photodiodes. Photodiode 46 detects fluorescence from the reference region 66, and photodiode 48 detects fluorescence from the sensing region 68. The optical filters 50 and 52 overlie the photodiodes, to pass the fluorescence radiation while rejecting other wavelengths, in particular the excitation radiation from the LED. The optical filters 50 and 52 may be an epoxy coating, a glass filter, or a polymeric-based sheet
20 material. Preferably, a prefabricated polymeric-based sheet material is used. The emissions from the LED 44 and the fluorescence emissions from the films 66 and 68 pass through holes 60 in the plate 54. Preferably, the film circles 66 and 68, the holes 60, and the active areas of the photodiodes 46 and 48 are all circles of similar diameter.

During nitric oxide sensing measurements, the substrates 62 and 64 and sensing region 68 and reference region 66 preferably are maintained at a temperature sufficient to reduce problems associated with moisture condensation. The heating of the substrate is achieved by passing electrical current through the four surface-mounted resistors 76. The temperature of the copper plate 54 is monitored by the thermistor 78, allowing the heating current through the resistors and temperature to be regulated. If moisture was eliminated from the gas flow by some means, e.g. chemical drying, water absorbing/ adsorbing substances, membranes, filters, foam sheets, etc., or prevented from condensing on the fluorescent film, such as by some surface treatment (a nitric oxide-permeable hydrophobic film or other approaches), then the sensor need not be heated.

The thin fluorescent films used in the nitric oxide sensor respond very rapidly to changes in nitric oxide concentration thereby providing the sensor with instantaneous response, as that term is defined herein. The sensor has a response time preferably less than or equal to 200 milliseconds, and most preferably less than or equal to 100 ms. Even faster response times may be preferable for certain applications.

Additional details concerning the present approach to component gas concentration sensing may be obtained by reference to the discussion of a similar oxygen sensor in Applicant's co-pending patent application Serial No. 09/630,398, incorporated herein in its entirety by reference. As will be clear to those of skill in the art, other types of nitric oxide concentration sensors may be used as long as they have an instantaneous response and are not sampling-based sensors. Also, the concentration of other component gases may be monitored using a meter similar to

the one illustrated in the present invention. For example, an oxygen sensor may be added or may be substituted for the nitric oxide sensor so as to construct a calorimeter in accordance with Applicant's co-pending patent application Serial No. 09/630,398.

In the simplest embodiment of the present invention, the nitric oxide
5 concentration sensor is provided on the side of the flow tube, and flow sensors are not provided. In this embodiment, instantaneous nitric oxide concentrations may be monitored during respiration providing a curve of nitric oxide concentrations. This data may be useful in the diagnosis and treatment of various diseases without obtaining flow data. In a more complicated, and preferred, embodiment of the present
10 invention, flow sensors as previously discussed are also included. The flow sensors allow for determination of many additional parameters, including many respiratory parameters such as flow rate, flow volume, lung capacity, and others. For example, by including flow sensors, the meter can be used as a spirometer. The peak flow, the forced vital capacity (FVC), and the forced expiratory volume during the first second
15 (FEV 1) may be derived from the collected data. The nitric oxide data, such as the time dependent concentration, may be combined with these parameters. A modified version of the present invention may also be used to determine functional residual capacity as explained in U.S. Patent Nos. 5,540,233 to Larsson et al and 5,957,128 to Hecker et al, both of which are incorporated herein by reference.

20 Referring now to Figure 5, a first alternative embodiment of a nitric oxide meter according to the present invention is generally shown at 90. This embodiment of the present invention differs from the previous embodiment in that the flow pathway or flow tube 92 is generally rectangular in cross-section. This illustrates that the flow tube does not necessarily have to be circular in cross-section.

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Referring now to Figures 6 and 7, a second alternative embodiment of a nitric oxide meter according to the present invention is generally shown at 100. This embodiment has a configuration similar to the configuration of the calorimeter described in Applicant's co-pending patent application Serial No. 09/630,398. Details of this embodiment may be obtained by referenced to the co-pending application. Basically, the meter 100 includes a body 102 with a mask 104 extending therefrom. A display 106 is arranged on one side of the body 102 and a combination control button and indicator light 108 is disposed on another side of the body 102. Referring to Figure 7, a cross-section of this embodiment is illustrated. Unlike with the previous embodiment, the flow pathway is not a straight through design. Instead, the respiration gases follow a path generally indicated by arrows A through G through the body 102 and mask 104 of the meter 100. The flow tube 110 is arranged perpendicularly to the flow of respiration gases to and from the mask 104. An inlet conduit 112 interconnects the mask 104 with the flow tube housing 114. Ultrasonic flow sensors 116 and 118 are arranged above and below the ends of the flow tube 110 so as to measure the flow coaxially. Unlike the embodiment of Figure 1 and 2, calculation of flow velocity does not require correction for the flow sensors being arranged at an angle to the flow. This embodiment also differs from the previous embodiments in that the nitric oxide sensor 120 is positioned adjacent the flow pathway but below the bottom end of the flow tube 110. A nitric oxide meter according to the present invention may also be constructed in accordance with the other embodiments of the calorimeter discussed in Applicant's co-pending application Serial No. 09/630,398, by substituting a nitric oxide sensor, as previously described, for the oxygen sensor used with a calorimeter. Other calorimeter designs that may be

modified according to the present invention are disclosed in U.S. Patent Nos. 4,917,108; 5,038,792; 5,178,155; 5,179,958; and 5,836,300, all to Mault, a co-inventor of the present application, are incorporated herein by reference.

As will be clear to those of skill in the art, it may be beneficial to provide a
5 nitric oxide meter which may be sanitarily used by multiple users without significant risk of transfer of germs. Referring again to Figure 2, the mask 14 may include a biological filter 15 disposed therein to prevent the transfer of biological materials into the body 12 of the meter 10 from the mask 14. One example of a biological filter material 15 is Filtrete® from 3M. The use of the biological filter material allows the
10 mask 14 and/or the filter material 15 to be changed between users so as to provide sanitation. Other approaches to providing sanitary respiratory devices are described in Applicant's co-pending patent application Serial No. 09/630,398.

Referring now to Figure 8, a third alternative embodiment of a nitric oxide meter according to the present invention is generally shown at 130. This embodiment
15 is also designed for use by multiple users while providing sanitation. It includes a disposable portion 132 and a reusable portion 134. The disposable portion includes a flow tube 136, which is generally cylindrical and of constant cross-section, extending perpendicularly from a respiratory connector such as a mask 138. A pair of openings 140 are disposed in the upper side of the flow tube 136 near opposite ends of the flow
20 tube. Extending downwardly within the flow tube from the openings 140 are ultrasonically transparent, sanitary barrier socks 142. Alternatively, the socks could be replaced with more rigid structures with ultrasonically transparent windows therein. A third opening 144 is disposed in the upper side of the flow tube and has a piece of sanitary barrier material 146 disposed therein.

The reusable portion 134 is configured to mate with the upper side of the flow tube 136. The reusable portion has an elongated arcuate body 135 with a pair of ultrasonic transducers 148 extending downwardly from the body 135 on posts 150. The ultrasonic transducers 148 and posts 150 are sized and positioned so as to enter
5 the openings 140 in the disposable portion 132 when the reusable portion 134 is mated therewith. When the two portions are coupled, the ultrasonic transducers 148 are positioned approximately in the center of the flow tube 136 within the sanitary barrier socks 142. The ultrasonic transducers 148 are preferably of the small, micromachined type and work as previously described. However, because they are
10 positioned within the flow tube itself, the pulses traveling between the ultrasonic sensors are coaxial with the flow and do not require correction based on ultrasonic pulses traveling at an angle to the flow. A nitric oxide sensor, as previously described, is also supported on the body 135 of the reusable portion 134, and is generally indicated at 152. It is sized and positioned so as to fit into the third opening
15 144 in the upper side of the flow tube so that it is in contact with the flow within the flow tube, but protected from biological contamination by the filter material 146. A display 154 may also be provided on the reusable portion 134. In this embodiment, the reusable portion 134 may be retained for multiple uses and users while the disposable portion is specific to an individual user. As explained in Applicant's co-
20 pending patent application Serial No. 09/630,398, the meter of Figures 6 and 7 may also include a disposable and a reusable portion.

Referring now to Figure 9, another embodiment of a nitric oxide meter according to the present invention is generally shown at 160. This embodiment is similar to the first embodiment of the present invention in that the meter 160 includes

a generally cylindrical flow tube 162 with the ultrasonic flow sensors being disposed in side passages angled to the flow tube. However, in this embodiment, a disposable insert 164 which includes a mouthpiece 166 and a sanitary sleeve 168. The sleeve portion 168 of the insert 164 slides into the flow tube 162 so as to line the flow tube.

5 The sleeve is ultrasonically transparent so that the ultrasonic flow sensors can monitor flow through the sleeve 168. A nitric oxide sensor 170 is disposed in the underside of the flow tube 162 so as to be in contact with flow through the sleeve 168. The sleeve is either porous to nitric oxide or includes a window having material that allows the passage of nitric oxide. As a further aspect of the present invention, data processing,
10 storage, and analysis may be performed by a remote computing device such as a personal digital assistant (PDA) 172. The PDA 172 is docked into an interface 174 which is wired to the sensor body. Alternatively, data may be transferred between the sensor and the PDA by wireless means or by transfer of memory modules which store data, as described in Applicant's co-pending patent application Serial No. 09/669,125,
15 incorporated herein in its entirety by reference. Also, the nitric oxide meter may communicate with other remote devices, such as stationary or portable computers and remote devices such as servers via the Internet or dock or interconnect with a PDA, as also described in the co-pending application. These alternatives apply to all embodiments of the present invention.

20 Referring now to Figure 10, an additional aspect of the present invention will be discussed. As explained in the Background, administration of nitric oxide to the respiratory system of a patient is beneficial in the treatment of some disorders. A system for the controlled administration of nitric oxide to a patient is generally shown at 200 in Figure 10. The system includes a respiration gas source 202 which is

interconnected with respiratory connector 204 by a conduit 206. The respiratory connector may be of any type, such as a mask or a connector for intubating the patient. A nitric oxide source 208 is also provided and is interconnected with the conduit 206 by a control valve 210. A nitric oxide meter 212 according to the present invention is disposed in the conduit 206 so that respiration gases mixed with nitric oxide flowing through the conduit 206 pass through the meter 212. A control system 214 is interconnected with the meter 212 and the control valve 210 so as to provide feedback control of the nitric oxide administration system. Meter 212 may be constructed according to any of the embodiments of the present invention and includes a nitric oxide sensor operable to determine the instantaneous concentration of nitric oxide in the respiration gases flowing through the meter. The output of the meter 212 is fed to the control system 214. The control system 214 then controls the control valve 210 so as to maintain the desired concentration of nitric oxide flowing through the conduit 206. As will be clear to those of skill in the art, the system 200 may be used with any of the approaches of administering controlled amounts of nitric oxide as described in the prior art. For example, pulses of nitric oxide may be administered to the patient rather than having continuous flow. The meter 212 is useful in determining the changing quantity of nitric oxide during such an administration procedure. As will be clear to those of skill in the art, the system 200 may also be configured as a forced respiration system for patients requiring assistance in respiration or as part of an anesthesia system. Alternatively, the nitric oxide meter 212 may monitor both inhalation and exhalation. In this case the meter is preferably very close to the connector 204 to minimize dead air space. Instead, two meters may be used.

As will be clear to those of skill in the art, various alterations may be made to the above-described embodiments of the present invention without departing from its scope or teaching. For example, the nitric oxide meters could include graphic displays to show profiles of nitric oxide, breath flow, or other parameters for a period
5 of time such as a single breath or one minute. Data may also be averaged over multiple breaths to provide an averaged profile. The meter, or other devices used with the meter, may include a memory and a processor to store flow profiles or nitric oxide profiles indicative of various physiological conditions including a healthy normal state and various physiological disorders. The meter or associated computational
10 device may then compare the patient's data with the stored profiles in order to make a preliminary diagnosis. A PDA may interconnect with the nitric oxide meter and provide the necessary display and processing as well as diagnosis. Other alternatives will also be clear to those of skill in the art. It is the following claims, including all equivalents, which define the scope of the present invention.

15 I claim:

1. A respiratory nitric oxide meter for measuring the nitric oxide content
2 of respiration gases for a subject, said meter comprising:
a respiratory connector configured to be disposed in fluid communication with
4 the respiratory system of the subject so as to pass the respiratory gases as the subject
breathes;
6 a flow pathway operable to receive and pass the respiration gases, the pathway
having a first end in fluid communication with the respiratory connector and a second
8 end in fluid communication with a reservoir of respiratory gases; and
a nitric oxide concentration sensor operable to generate electrical signals as a
10 function of the instantaneous fraction of nitric oxide in the respiration gases as the
gases pass through said flow pathway.
2. The respiratory nitric oxide meter according to claim 1, wherein the
2 respiratory gases are exhalation gases.
3. The respiratory nitric oxide meter according to claim 1, wherein the
2 respiratory gases are inhalation gases.
4. The respiratory nitric oxide meter according to claim 1, wherein the
2 respiratory gases are inhalation gases and exhalation gases
5. The respiratory nitric oxide meter according to claim 1, wherein said
2 flow pathway comprises a generally cylindrical flow tube and said nitric oxide sensor
is supported on said tube.

6. The respiratory nitric oxide meter according to claim 5, wherein said
2 flow tube has a side wall with an opening defined therein and said nitric oxide sensor
is at least partially disposed in said opening.

7. The respiratory nitric oxide meter according to claim 1, wherein said
2 nitric oxide sensor is a fluorescence based sensor.

8. A respiratory nitric oxide meter for measuring the nitric oxide content of
2 respiration gases for a subject, said meter comprising:

a respiratory connector configured to be disposed in fluid communication with
4 the respiratory system of the subject so as to pass the respiration gases as the subject
breathes;

6 a flow pathway operable to receive and pass the respiration gases, the pathway
having a first end in fluid communication with the respiratory connector and a second
8 end in fluid communication with a reservoir of respiratory gases;

a flow meter configured to generate electrical signals as a function of the
10 instantaneous flow of respiration gases passing through said flow pathway; and

a nitric oxide concentration sensor operable to generate electrical signals as a
12 function of the instantaneous fraction of nitric oxide in the respiration gases as the
gases pass through said flow pathway.

9. The respiratory nitric oxide meter according to claim 8, wherein the
2 respiratory gases are exhalation gases.

10. The respiratory nitric oxide meter according to claim 8, wherein the
2 respiratory gases are inhalation gases.

11. The respiratory nitric oxide meter according to claim 8, wherein the
2 respiratory gases are inhalation gases and exhalation gases.

12. The respiratory nitric oxide meter according to claim 8, wherein said
2 flow meter comprises an ultrasonic flow meter including a pair of spaced apart
ultrasonic transducers.

13. The respiratory nitric oxide meter according to claim 12, further
2 comprising a pair of side passages intersecting said flow pathway, said side passages
aligned with each other and extending from said flow pathway at an angle, said
4 ultrasonic transducers being disposed in said side passages.

14. The respiratory nitric oxide meter according to claim 12, wherein said
2 flow pathway comprises a generally cylindrical flow tube having a central axis and
said ultrasonic transducers are generally aligned with said central axis such that pulses
4 traveling between said transducers travel along a path coaxial with said flow tube.

15. The respiratory nitric oxide meter according to claim 8, wherein said
2 meter comprises a disposable portion including said respiratory connector and said
flow pathway and a reusable portion including said flow meter and said nitric oxide
4 concentration sensor.

16. The respiratory nitric oxide meter according to claim 15, wherein said
2 flow pathway comprises a generally cylindrical flow tube with openings for receiving
said flow meter and said nitric oxide concentration sensor.

17. The respiratory nitric oxide meter according to claim 8, wherein said
2 flow pathway comprises a flow tube having a side wall with an opening defined
therein and said nitric oxide sensor is at least partially disposed in said opening.

18. The respiratory nitric oxide meter according to claim 8, wherein said
2 nitric oxide sensor is a fluorescence based sensor.

19. A system for the controlled administration of nitric oxide to a subject,
2 said system comprising:

a respiratory connector configured to be disposed in fluid communication with
4 the respiratory system of a subject so as to pass inhalation gases as the subject
breathes;

6 a flow pathway operable to receive and pass the inhalation gases, the pathway
having a first end in fluid communication with the respiratory connector and a second
8 end in fluid communication with a source of respiratory gases;

a nitric oxide regulator operable to selectively introduce nitric oxide into the
10 inhalation gases in the flow pathway, said regulator in fluid communication with a
source of nitric oxide; and

12 a nitric oxide concentration sensor operable to generate electrical signals as a
function of the instantaneous fraction of nitric oxide in the inhalation gases as the
14 gases pass through said flow pathway.

20. The system according to claim 19, further comprising a controller
2 operable to receive said electrical signals from said concentration sensor and
operative to control said nitric oxide regulator such that the instantaneous fraction of
4 nitric oxide in the inhalation gases in said flow pathway remains within predetermined
limits.

21. The system according to claim 19, further comprising a flow meter
2 operable to generate electrical signals as a function of the instantaneous flow of
inhalation gases through said flow pathway.

22. The system according to claim 21, wherein said flow pathway includes
2 a generally cylindrical flow tube, said nitric oxide sensor being at least partially
disposed in said flow tube such that said sensor is in contact with the inhalation gases
4 passing through said flow tube.

23. The system according to claim 22, wherein said flow meter is
2 supported by said flow tube and operable to measure flow velocity in said flow tube.

24. The system according to claim 21, wherein said flow meter comprises
2 an ultrasonic flow meter including a pair of spaced apart ultrasonic transducers.

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FIG-1

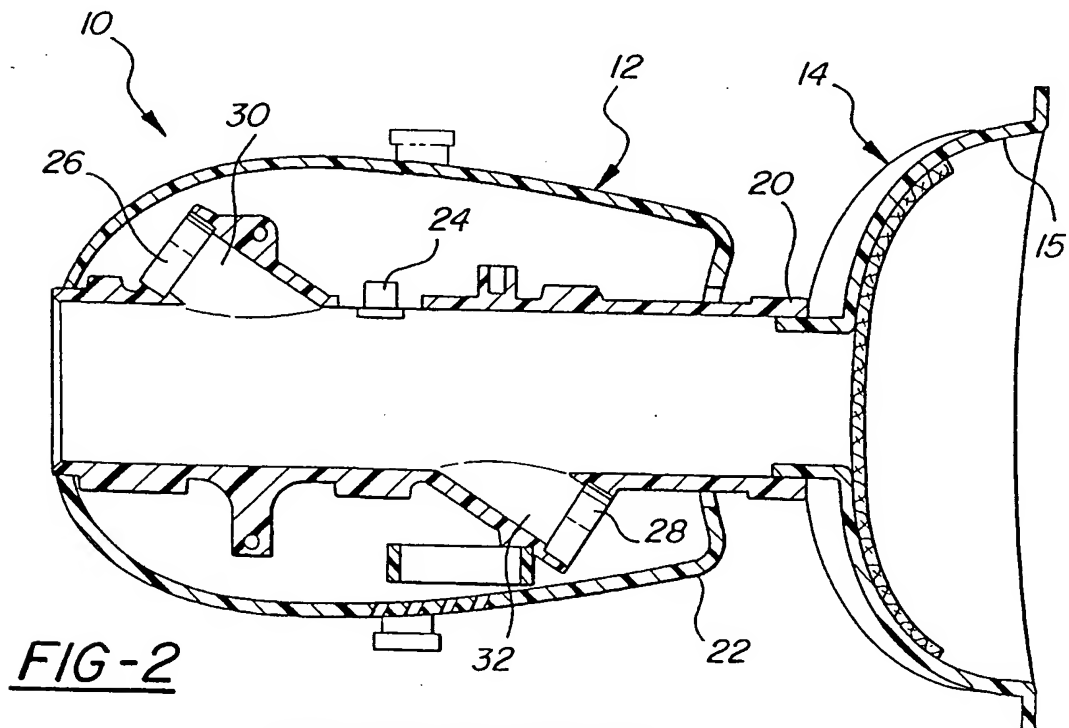
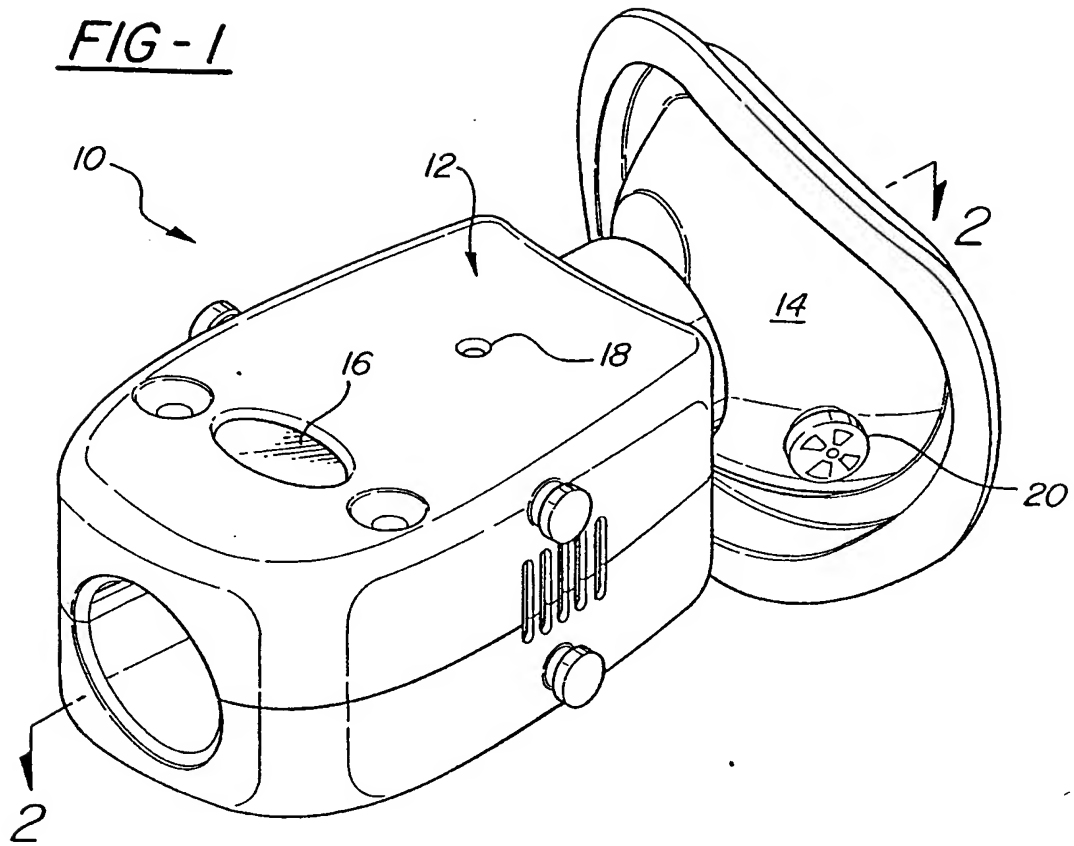
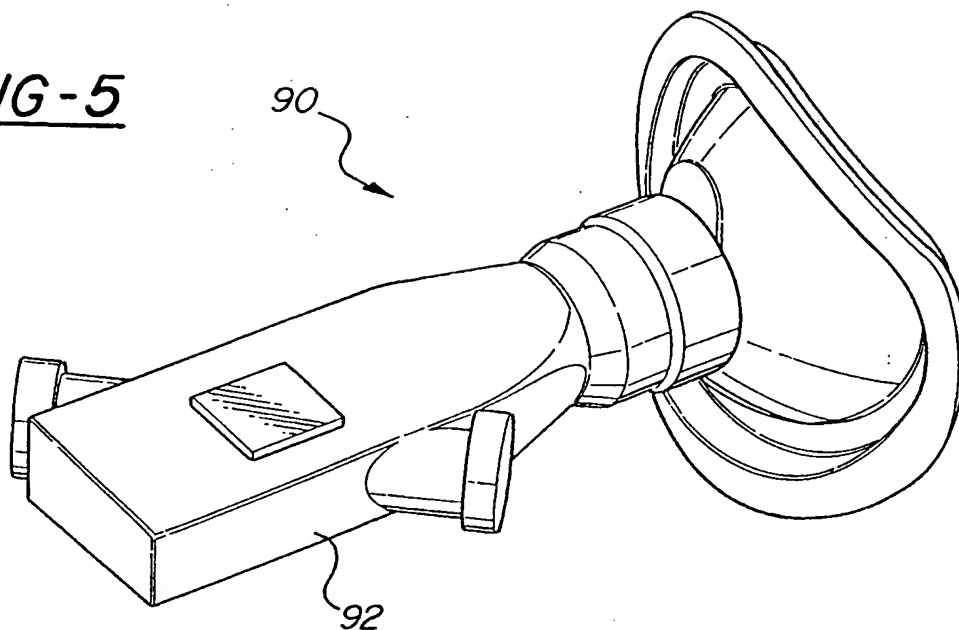
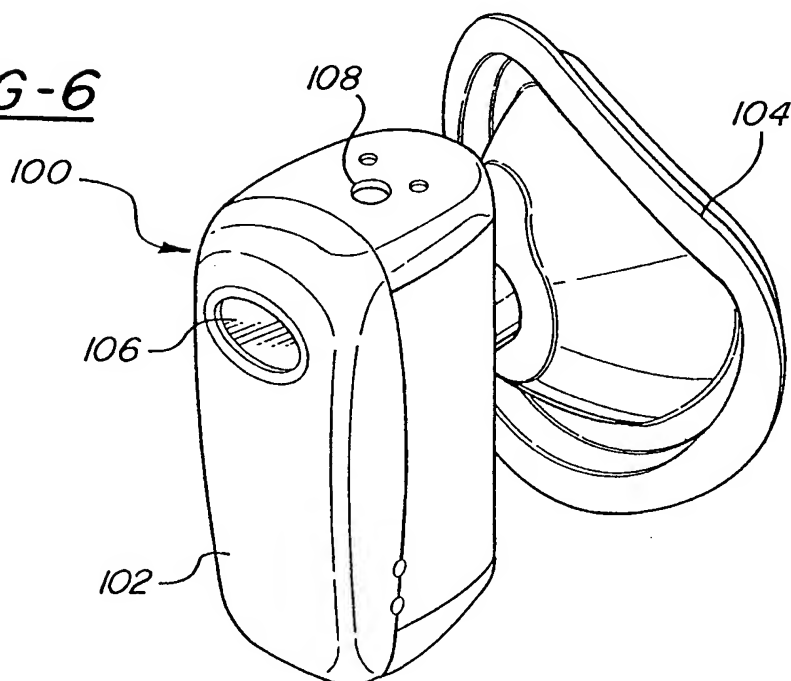


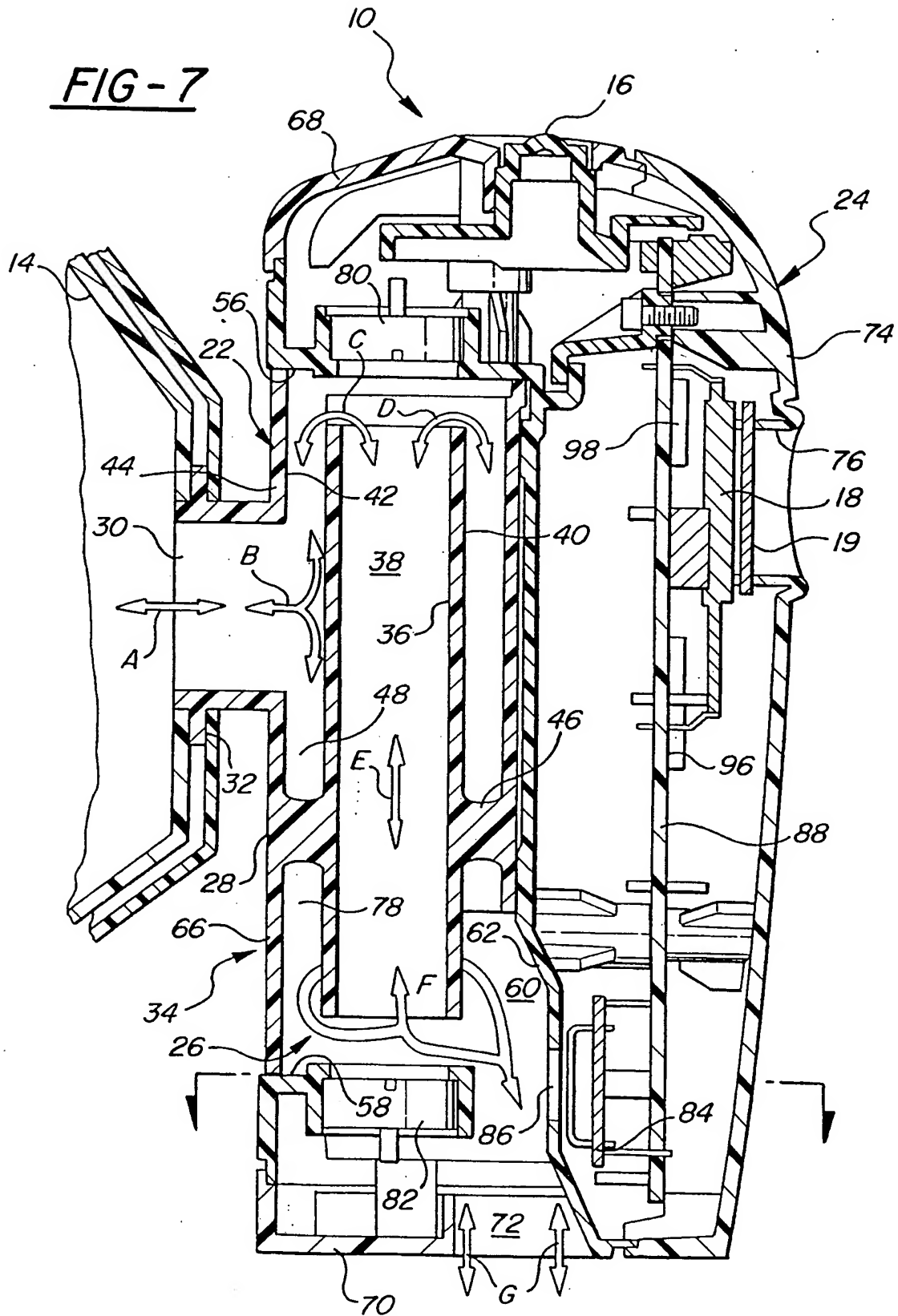
FIG-2

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FIG-5FIG-6

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FIG - 7



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FIG-8

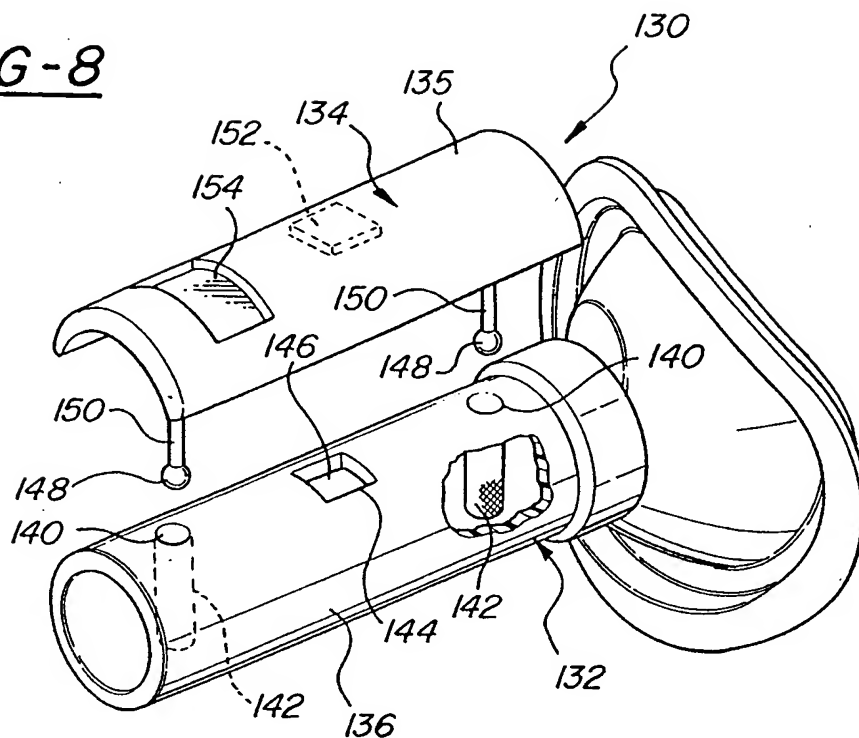
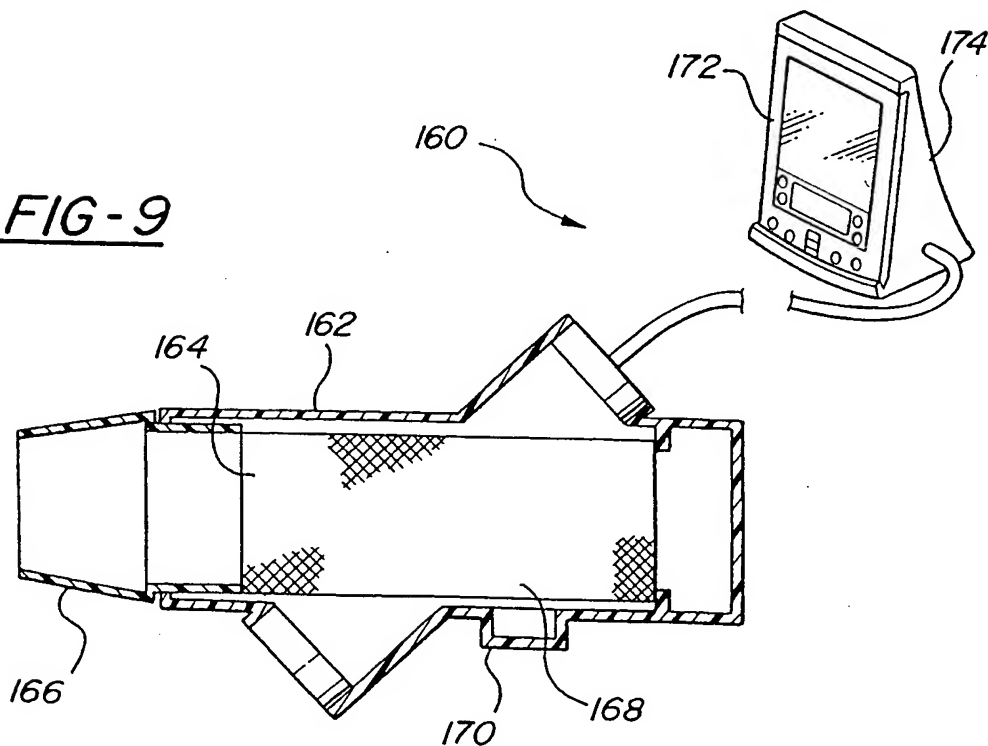


FIG-9



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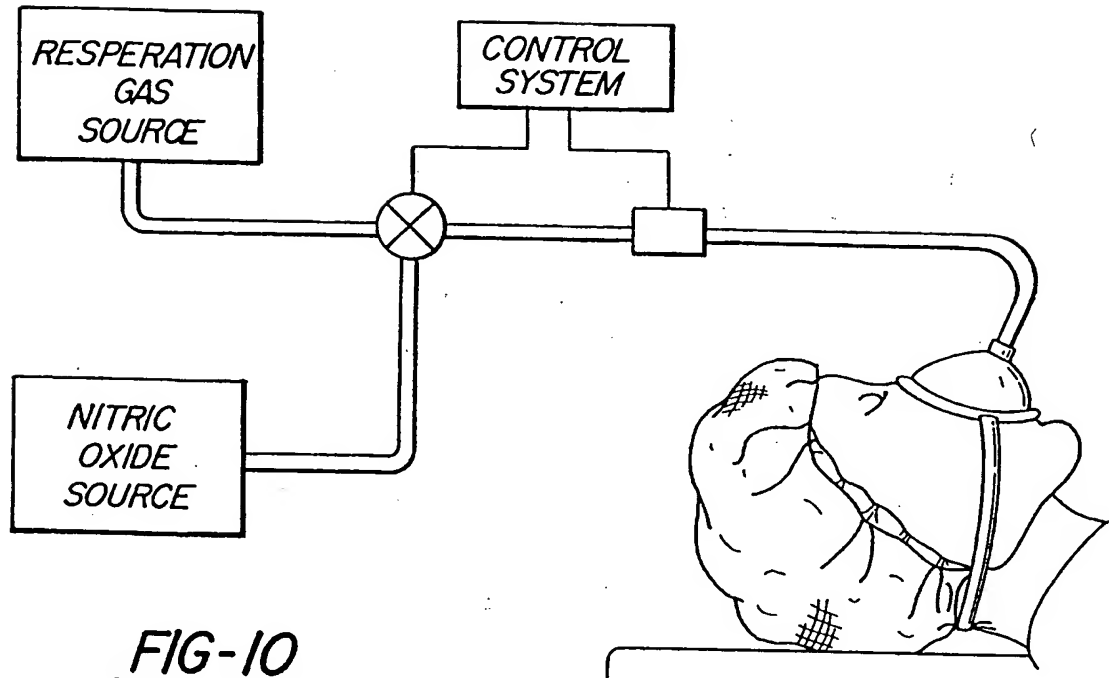


FIG-10

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US00/28220

A. CLASSIFICATION OF SUBJECT MATTER

IPC(7) : A61B 5/08

US CL : 600/532

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 600/532, 529, 538; 128/200.24

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
NONEElectronic data base consulted during the international search (name of data base and, where practicable, search terms used)
NONE**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5,309,921 A (KISNER et al.) 10 May 1994, see entire document.	1-24
A	US 5,326,973 A (ECKERBOM et al.) 05 July 1994, see entire document.	1-24

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

Special categories of cited documents:	
"A" document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E" earlier application or patent published on or after the international filing date	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
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"O" document referring to an oral disclosure, use, exhibition or other means	"&" document member of the same patent family
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

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